

Supplementary Materials for

Bioinspired mechanically active adhesive dressings to accelerate wound closure

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Other Supplementary Material for this manuscript includes the following:

(available at advances.sciencemag.org/cgi/content/full/5/7/eaaw3963/DC1)

Movie S1 (.mp4 format). Finite element simulation of AAD-enabled wound contraction.

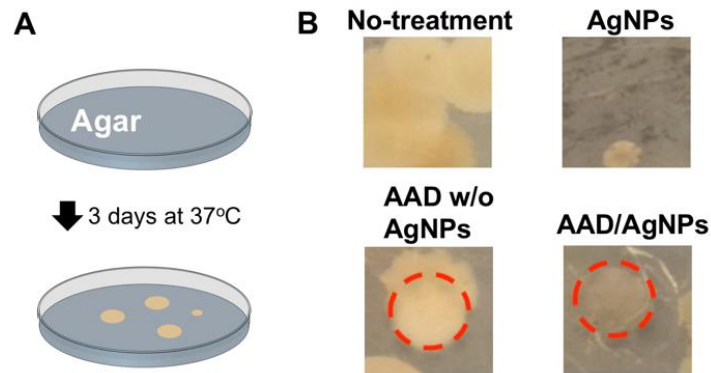


Fig. S1. Antimicrobial tests. (A) Schematics of the antimicrobial tests. (B) Digital images of the surface of agar gels with different treatments. The location of AAD without and with silver nanoparticles (AgNPs) is marked with a red dashed circle.

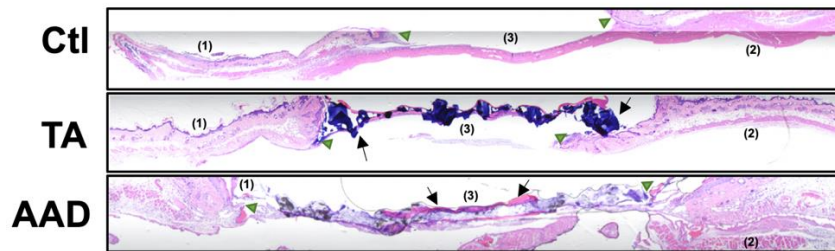


Fig. S2. Histological sections on day 3 specimens. The wound was treated with Tegaderm[®] as a control, tough adhesives (TA), or AAD. The wounded skin was harvested on Day 3 and H&E stained. The wound edges and the residues of adhesives are labeled with green triangles and black arrows, respectively. The epidermis, dermis, and wound bed are marked with (1), (2), and (3), respectively.

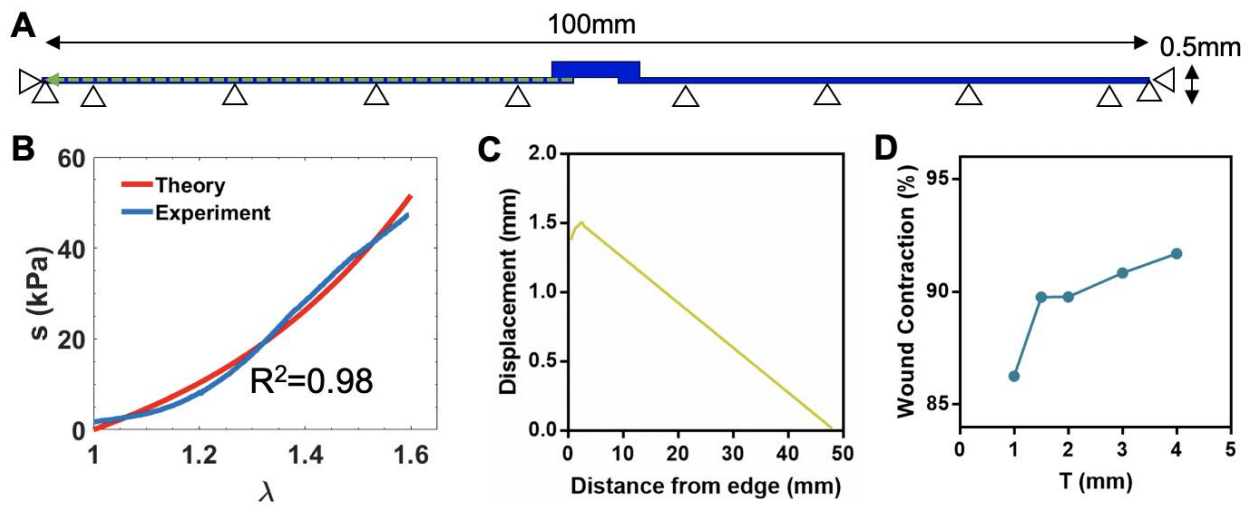


Fig. S3. Finite element simulation. (A) Configuration and boundary conditions of the simulation. The distance from wound edge is measured along the green dashed arrow. (B) Stress-strain curve of rodent skin fitted with Ogden model up to stretch ratio λ of 1.6. The nominal stress s is defined by the force divided by the initial cross-sectional area. (C) Horizontal displacement of the skin elements in the middle plane as function of the initial distance from the wound edge. (D) Wound contraction as a function of the adhesive thickness (T).

Table S1. Material parameters used in finite element stimulation. The Ogden parameters (μ , α) of rodent skin was experimentally measured and fitted in fig. S3B. The parameters of AAD, except the shear modulus (G), were cited from Cai and Suo (2014) (19), including cross-link density (N_v), initial swelling ratio with respect to the dry state (λ_0), initial temperature (T_0), triggered temperature (T_F), the parameters (A_0 , B_0 , A_1 and B_1) used to formulate the Flory-Huggins coefficient (χ) as a function of temperature (T) and the polymer fraction (ϕ) via equation, $\chi=(A_0+B_0T)+(A_1+B_1T)\phi$. Sample size $n=5$. G was calculated by one third of elastic modulus measured by tensile tests.

Rodent skin		AAD								
μ (kPa)	α	G (kPa)	N_v	λ_0	T_0 (K)	T_F (K)	A_0	B_0	A_1	B_1
25.90 (16.9-34.8)	7.08 (6.59-7.58)	4.66	0.01	2.36	280	310	-12	0.042	17	-0.057

Table S2. Comparison of mechanical and antimicrobial properties of materials related to wound care. The AAD and TA are compared with existing products related to wound care, including skin graft (36), ALGICELL[®] (Derma Sciences) (17), Band-Aid[®] (Johnson & Johnson), Tegaderm[®] (3M) (37,38), COSEAL[®] (17) and TISSEEL[®] (Baxter) (39), and Dermabond[®] (Ethicon) (17).

Products	Materials	Adhesiveness (Jm ⁻²)	Toughness (Jm ⁻²)	Active closure (2D strain %)	Antimicrobial	
AAD	Alginate-PNIPAM	200	2000	64%	√	
TA	Alginate-PAAm	1200	18000	0	×	
Wound dressings	Skin graft ^{2*}	Skin	5-40	>8000	0	×
	ALGICELL [®]	Alginate	3	5	0	√
	Band-Aid [®]	Acrylate/fabric	1-10	10000	0	×
	Tegaderm [®]	Acrylate	20-40	2000	0	×
Tissue adhesives	COSEAL [®]	PEG	30	30	0	×
	TISSEEL [®]	Fibrin	60	60	0	×
	Dermabond [®]	Cyanoacrylate	300	2000	0	×